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INVESTIGATION OF PHOTOBIOSTIMULATORY EFFECT OF 670NM DIODE LASER ON MRC-5 FIBROBLASTS (HUMAN FETAL LUNG) PROLIFERATION

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M.Sc. THESIS BIOMEDICAL ENGINEERING PROGRAMME

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T.C. FATİH ÜNİVESİTESİ BİYOMEDİKAL MÜHENDİSLİK ENSTİTÜSÜ

670 NM DİYOT LAZERİN MRC-5 (İNSAN FETAL AKCİĞER) FİBROBLAST HÜCRELERİNİN ÇOĞALIMI ÜZERİNDEKİ FOTOBİYOUYARICI ETKİSİNİN ARAŞTIRILMASI

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İSTANBUL, NISAN / 2016

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FATIH UNIVERSITY INSTITUTE OF BIOMEDICAL ENGINEERING

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This work is dedicated to Zainab, my wife, contant companion, and best friend for three years of marriage. She is the loving mother of my children: Lubna (Aisha) and Hidaya (Yahanasu), she has demonstrated incredible patience and understanding with rather painful process of this research while maintaining a most pleasant, cheerful and comforting home while my love to her keep increasing daily, thank Allah the Almighty for your blessings to our marriage.

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LIST OF SYMBOLS

- λ Lambda (Wavelength)
- Registered sign
- TM Trade mark sign
- Degree sign
- μ Micro sign
- α Alpha sign
- β Beta sign

ABBREVIATIONS

ADP	: Adinosine Diphosphate
ADSCs	: Adipose-Derived Mesenchymal Stem Cells
ALP	: Alkaline Phosphate
ATP	: Adenosine Triphosphate
BMSCs COX	: Bone Marrow Mesenchymal Stem Cells : Cytochrome c oxidase
CO_2	: Carbon Dioxide
DMSO	: Dimethyl Sulfoxide
DNA	: Deoxyribo Nucleic Acid
ECM	: Extracellular Matrix
EMEM	: Eagle's Minimum Essential Medium
ETC	: Electron Transport Chain
FBS	: Fetal Bovine Serum
FCS	: Fetal Calf Serum
GaAlAs	: Gallium Aluminum Arsenide Laser
LED	: Light Emitting Diode
LLLI	: Low Level Laser Irradiation
LLLT	: Low Level Laser Therapy
MRC-5	: Human Fetal Lung Cells
NADH ⁺	: Nicotinamide Adenine dinucleotide Reduced
NADPH	: Nicotinamide Adenine dinucleotide Phosphate Reduced
NIR	: Near Infrared
NO	: Nitric Oxide
O_2	: Oxygen
PBS	: Phosphate Buffered Saline
RNA	: Ribonucleic Acid
ROS	: Reactive Oxygen Species
UV	: Ultra Violet
XY	: Normal Diploid Male

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SUMMARY

INVESTIGATION OF PHOTOBIOSTIMULATORY EFFECT OF 670NM DIODE LASER ON MRC-5 FİBROBLASTS (HUMAN FETAL LUNG) PROLIFERATION

Nuhu Muhammad ABUBAKAR

Biomedical Engineering Programme

M.Sc. Thesis

Advisor: Assist. Prof. Dr. Haşim Özgür TABAKOĞLU

Low Level Laser Therapy (LLLT) has been shown to be effective in a variety of medical conditions such as healing processes exerting a positive photobiostimulatory effect due to its ability to promote cell proliferations. In this study, the MRC-5 human fetal lung fibroblast was submitted to three applications of low level laser irradiation (670nm, power 10, 50 and 100 mW with 1.58J/cm²). WST-1 assay was used to to evaluate cell viability, and growth curves were used to analyaze proliferation at 3, 6 and 24 hours. MRC-5 human lung fibroblast responded to LLLT in power-dependant manner. Higher cells proliferation was observed in the group irradiated with power of 50 mW at 3 and 6 hours. Mean proliferation rate for all treatment groups were found to differ significantly from the control groups with lower mean value (p>0.05) from the control than tests. No statistical significant difference (p>0.05) was found between compared 10 & 100 mW, 10 & 100 mW and 50 & 100 mW in 3, 6 and 24 hours respectively. Therefore, LLLI stimulate the proliferation of MRC-5 more effectively with 50 mW power especially at 3 hours as evidenced by increase in cell numbers as observed in the growth curves. The biostimulation of MRC-5 fibroblasts using laser therapy may be an important tool in regenerative or healing therapy.

Keywords: LLLT, Cell Proliferation, MRC-5 Fibroblast, Cell Viability, 670nm Diode.

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670 NM DİYOT LAZERİN MRC-5 (İNSAN FETAL AKCİĞER) FİBROBLAST HÜCRELERİNİN ÇOĞALİMİ ÜZERİNDEKİ FOTOBİYOUYARİCİ ETKİSİNİN ARASTİRİLMASİ

Nuhu Muhammad ABUBAKAR

Biyomedikal Mühendisliği Programı Yüksek Lisans Tezi

Danışman: Yrd.Doç. Dr. Haşim Özgür TABAKOĞLU

Düşük Seviye Lazer Terapisinin hücre çoğaltımını sağlayıcı foto-biyo uyarıcı özelliği, bu terapinin iyileşme ile ilgili birçok medikal vakada etkili olduğunu göstermiştir.

Çalışmamızda, MRC-5 insan cenin akciğer fibroblastı deneysel tüm uygulamalarda kullanıldı (3, 6 ve 24 saatlik) Lazer uygulama parametreleri : 670nm, 1.58 J/cm2 ile güç 10, 50 ve 100 mW olarak belirlendi. Hücre canlılığını değerlendirmek için WST-1 analizi kullanıldı. Gelişim eğrileri çoğalmanın 3, 6 ve 24 saatlerde analizi için kullanıldı. MRC-5 insan akciğer fibroblastları DSLT'nin gücüne bağlı olarak tepki verdi. Daha yüksek hücre çoğalması 3 saat 50 mW'lık gücün uygulandığı grupta gözlemlendi. Ortalama çoğalma oranının tüm uygulama grupları için daha düşük ortalama seviyesine sahip kontrol gruplarından (p>0.05) istatistiksel olarak farklı olduğu bulgulandı. Sırasıyla 3, 6 ve 21 saatlik 10&100 mW, 10&100 mW ve 50&100 mW uygulamalarıı arasında belirgin istatistiksel bir farklılık ortaya çıkmadı (p>0.05). Böylelikle, 50mW güçte özellikle 3 saatlik DSLT uygulaması MRC-5 çoğalmasını sağladığı, çoğalma eğrilerinde hücre sayısında artışın gözlemlenmesiyle tespit edilmiştir. MRC-5 fibroblastların lazer terapiyi kullanarak biyo-uyarımı, doku yenilenmesi veya yara iyileştirme terapilerinde önemli bir araç olarak kullanılabilir.

Anahtar kelimeler: DSLT, Hücre Çoğalması, MRC-5 Fibroblast, Hücre Canlılığı, 670nm Diyot.

FATİH ÜNİVERSİTESİ -BİYOMEDİKAL MÜHENDİSLİK ENSTİTÜSÜ

CHAPTER 1

1.1 Purpose of the Thesis

Laser (Light amplification by stimulated emission of radiation) is a device that simply generates electromagnetic radiations which are relatively uniform in wavelength, phase, and polarization, which was demonstrated in 1960 by a scientist called Theodore Maiman in the form of a ruby laser [1]. Typically we can define laser as a source of light or as radiation energy [2]. Low Level Laser (LLL) is a inique device that is used as biostimulatory tool which exert its effects on biologic systems on the bases of nonthermal means [3]. This interesting area of investigation was initiated since 1067 by Mester et al. who put their efforts in this regard. They reported non-thermal effects of laser on mouse hair growth [4]. Low level laser irradiation (LLLI) is used in several researches to stimulate different types of cells proliferation and differentiation [4-8]. However, sometimes the photo-biostimulation is not always effective due to the different types of factors that may influence the process [9]. Thefore, for this reason in vitro biostimulation depends on laser-related parameters such as wavelength, dose, power and time of irradiation [7, 8, 10], type of cells irradiated [11], and the physiological characteristics of the cells at the time of irradiation [8, 10]. So as a consequence of these factors, the interaction of laser light with cells and tissues can stimulate or inhibit cell proliferation.

The present study aims to evaluate a possible photo-biostimulatory influence of low level laser irradiation on MRC-5 Fibroblasts (Human Fetal Lung) cell line proliferation in a systematic manner. The experiment was designed to access the following individual objectives:

1.2 Objectives:

The individual objectives of this research include the followings:

- 1. To evaluate cell proliferation rate among the treatment and control groups.
- 4. To make statistical comparison among the treatment and control groups.

3. To find out the possible best therapeutic mode of 670nm diode low level laser irradions power.

1.3 Motivation

MRC-5-fibroblasts (human fetal lung) are undifferentiated cells with important potential for applications in cell therapy because of their capacity for self-renewal, proliferation, and differentiation into diverse types of specialized cells. The MRC-5 cell line was developed in September 1966 from lung tissue taken from a 14 week fetus aborted for psychiatric reason from a 27 year old physically healthy woman. The cell morphology is fibroblast-like. The karyotype is 46, XY; normal diploid male. Cumulative population doublings to senescence is 42-48. G6PD isoenzyme is type B. Studies have shown that the higher the proliferation of the cells, the greater the regenerative and healing capacity of the tissues where they reside.

According to the authors, *in vitro* studies normally reflect the same conditions as observed in open wounds, i.e., the lack of an optical barrier, and lower doses are, thus, indicated in the case of cells biostimulation.

Health clinicians seek optimal methods of promoting wound healing, however this remains a challenge all over the world. Wound and injuries presents a dilemma of global proportions and attract great clinical interest due to high morbidity attributed to changes in the normal healing process [12]. Economically, chronic wound management has been reached a total cost of 2-4% of the health budget in western countries [12] and that the annual expenditure on wound and injuries related problems in the USA alone exceeds one billion dollars [13]. Complications in non-healing wounds are vast, and patients are at risk of severe pain, septicaemia, hospitalization, and in some cases amputations [14].

Furthermore, these changes may also inflict increased cost to society, and reduce quality of life for a huge number of peoples worldwide. The idea of effective therapeutic strategies and cheap alternatives that might work in the healing process attracts much attention [15]. Indirectly, this research will contribute to the enhancement of the recovery and lead to shorter stay in health care facility (reduced nosocomial infections),

reduced cost of wound care, and enhanced quality of life for patients suffering from wound related problems as well as faster return to routine activities.

Additionally, LLLI has been shown to stimulate the growth, proliferation and differentiation of different types of cells in culture, including keratinocytes, fibroblasts, endothelial cells, myoblasts, and osteoblasts, by exerting positive biomodulatory effects[16, 17]. However, little is known about the effect of laser therapy on MRC-5 because the proliferation of MRC-5 is usually slow and the yield of these cells after first harvest is low, a therapeutic tool that increases their proliferation without causing molecular damage while maintaining their specific characteristics is important for effective clinical application of these cells.

The laser radiation produces many different effects depending on light-beam parameters as well as the tissues that are subjected to irradiation. Despite documented therapeutic effect of low-level laser therapy (LLLT), there is still much controversy and scientific debate over its effectiveness on different cells[18-20].

The variety of procedures and the inconclusive results of the conducted studies mobilized to search for the parameters of laser radiation, which both in vitro and in vivo will result in acceleration of cell proliferation and the expected therapeutic efficacy. The relevance of some irradiation parameters remains occult and represents an important area for further research and repeated treatments are necessary to achieve a positive laser effect in clinical applications. This draws my attention to make a further study in order to optimize irradiation parameters by assessing the MRC-5 Fibroblasts (Human Fetal Lung) proliferations.

3

CHAPTER 2

2.1 Cells

The living things are composed of cells which exist in different, ranging from single cell organisms that practice free living to those in complex biological organisms like human. All the biological living systems despite the great diversity exhibited between them, remarkably, are composed of the same types of chemical molecules and apply similar principles in metabolism and replication, in higher organisms such as human, they have the ability to organize at the cellular levels [21, 22].

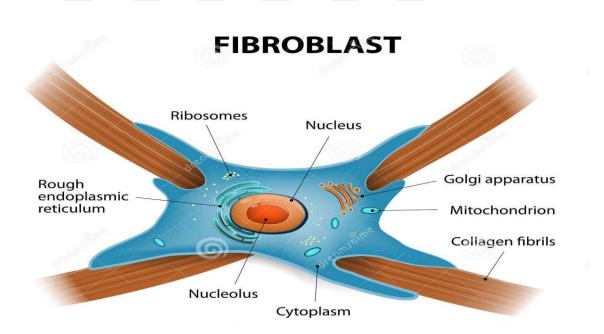


Figure 2.1 Structure of Fibroblast [23]

Regarding the internal structures and organelles of the cell, thus serve as biological system that are essentially an assembly of molecules where water, amino acids, carbohydrates (sugar), fatty acids, and ions account for 75–80% of the matter in cells, the remaining 25–20% cell mass are macromolecules [24].

2.2 Mechanism of Cell Proliferation

Cell proliferation lead to the productions of two daughter cells from single one, this is achieved through cell growth followed by cell division. Cell proliferation as observed in normal tissue is generally restricted to cells that replenish the tissue. Proliferation depends on availability of tissue-type specific growth factors, which are signals, not nutrients. Proliferation requires interaction of transmembrane proteins called integrins with components of the extracellular matrix (ECM) components. Contact inhibition of growth limits division in culture when cells form a contiguous monolayer. For human fibroblasts divide a limited number of times (ca. 50-70 divisions for human cells) before the cells enter a senescent state that maintains metabolic activity but stops all further division [25].

2.2.1 Cell Cycle

Cell division occurs in defined stages, which together comprise the cell cycle. In terms of the genetic material, cells must replicate their chromosomal DNA once every cell cycle and segregate the sister chromatids produced by DNA replication to yield two genetically identical daughter cells [26].

Molecular mechanisms induced by laser radiation involved mitochondrial photoacceptors and production of Reactive Oxygen Species (ROS) [27–30]. Furthermore, laser radiation might affect cell cycle progression, protein synthesis, cell energy metabolism, proliferation and apoptosis by modulation of specific kinases and phosphatases [28, 31, 32]. The effect of laser radiation on cell growth, cell cycle progression and apoptosis has been widely studied and compared to the effect produced on non-irradiated cells by the use of many different Sources (generally low power lasers), wavelengths (mostly red and NIR radiation), energy doses (from tenths to tens of J/cm²) and treatment modes.

2.2.2 Stages of Cell Cycle during Cell Proliferations

The cell division cycle is broken up into four stages: G1, S, G2 and M (Figure3). DNA replication occurs during S ("synthesis") phase [26]. DNA packaging, chromosome segregation and cell division (cytokinesis) occur in M (mitosis). S phase and M phase are separated by Gap phases. G1 is the gap between M and S. Cell growth is one of the important events of G1. The transition from G1 to S is the critical control point in the cell cycle. G2 is the gap between S and M, and provides time for proofreading to ensure DNA is properly replicated and packaged prior to cell division. G0 or quiescence occurs when cells exit the cell cycle due to the absence of growth-promoting signals or presence of pro-differentiation signals. The G1, S, and G2 phases comprise interphase, which accounts for most of the time in each cell cycle [26].

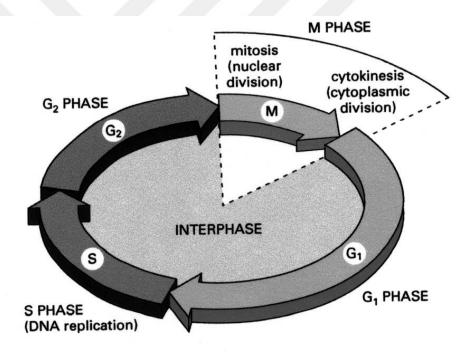


Figure 2.2 Demonstration of cell cycle stage [26]

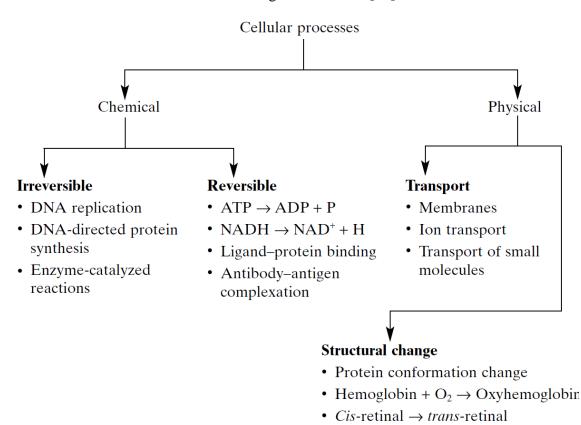
2.3 Cellular Processes

Physical and chemical changes are those processes that are involved in cellular processes [21]. However, chemical changes can result in permanent products (such as synthesis of protein, replication of DNA) or can be cyclic or reversible (like in conversion of ATP to ADP and back). The type of chemical changes that are taking

place are of highly complex, which are often accelerated by enzymes (proteins) and coenzymes (NADH). Table 2.1 showed different cellular processes that occur in cells [21].

 Table 2.1 Tissue, Cellular and Molecular Components that make ineteraction with Light

 when the light strike them [21]



2.4 Light-Induced Cellular Processes

Cells undergo different photophysical and photochemical processes during light absorption. Some of these processes are amount of cellular constituents fluoresce when excited directly or excited by energy transfer from another constituent [33]. Photochemical processes involving a chemical reaction in the excited state of a cellular constituent are varied [34, 35]. These chemical reactions that occur within the cellular membrane include the followings: (i) *Photoaddition*. In this process, UV-induced molecular lesions in the structure of DNA, an example of this process is photodimerization of thymine process responsible for.

(ii) *Photofragmentation*. In photofragmentation reaction, the original molecule when photoexcited, decomposed into smaller chemical fragments by the cleavage of a chemical bond. This type of reaction is very common in biomolecules when exposed to short wavelength UV light. An example is the photofragmentation of riboflavin.

(iii) *Photooxidation*. The main important point here is that, when excited molecule adds an oxygen molecule from the surroundings (a chemical process called oxidation). Photooxidation of cholesterol is one of the examples.

(iv) *Photohydration*. This process involved the creating of lesions in DNA in which an excited molecule adds a water molecule to produce a new product, as occur in uracil.

(v) *Photoisomerization*. This reaction involved the change in geometry or conformation of stereoisomers. This process account for retinal vision is that of 11-*cis*-retinal which upon excitation rotates by 180° around a double bond to produce a geometric isomer, the all *trans*- retinal.

(vi) *Photorearrangement*. In this process of photo-inducing, chemical formula of the molecule does not change, but bonds rearrangements take place as can be illustrated for 7-dehydrocholesterol in skin which upon UV exposure produces vitamin D3 [34, 35].

2.5 LLL Effect on Mitochondrial Cytochrome C Oxidase

Different studies shows mechanism of LLLT effects inevitably involve mitochondria, a main organelle for energy generation and metabolism via oxidative phosphorylation. Low level laser therapy (LLLT) induced processes that confirmed cellular physiologic activities. Many researches revealed the potentials of LLLT to trigger the mitochondrial respiratory chain. Cytochrome c oxidase (Cox), an enzyme that involved in transferring electrons between complexes III and IV of the electron transport chain (ETC) accompanying by near-infrared light stimulation [36, 37, 38]. Absorption spectra of Cox at different oxidation states were similar to that for biological responses to light [39].

This finding result into the proposal of Cox becoming the photoacceptor for the red to NIR range in human cells [39].

Therefore, stimulation of Cox leads to increased transfer of electrons and enhanced regulation of oxidative phosphorylation thus production of more ATP molecules [40, 41]. Recent studies also mentioned that under physiological conditions nitric oxide regulate Cox activity via reversible inhibition of mitochondrial respiration [42].

2.6 LLLT Mechanism of Actions

For Photo-biostimulatory effect of LLLT to occur and to have effect on living biological system, photons must be absorbed by electronic absorption bands of some molecular photoacceptors, or chromophores [43].

The cellular mechanism of LLLT has been linked to monochromatic visible and NIR radiation absorption by components of electron transport chain [44]. Mitochondrion is a core organelle responsible for cellular response to red and NIR light. LLL effects on rat liver mitochondria resulting the enabcement of proton electrochemical potential, increased ATP, NADH, RNA and protein synthesis [45, 46] and elavate membrane potential, and oxygen intake.

Several studies [47-50] support that cellular mechanism of LLLT on the bases of increased mitochondrial oxidative metabolism which caused by excitation of electronic components of the respiratory chain.

There have been four stages of Cellular mechanism of LLLT effect designated as primary, secondary, and tertiary [51, 52]. Generally, Primary reactions involved reactions due to photon absorption while secondary effects is not related to LLLT and their occurrence depended on cell sensitivity which differ from the primary. Tertiary (systemic) effects are affected by both internal and external environment including intracellular interactions as clearly reported why the treatment of one lesion can also stimulate healing in other lesions present [53].

2.6.1 Primary Effect of Light to Cells

Laser beams exert its effect on mitochondria [54] and cell membranes of fibroblasts, keratinocytes and endothelial cells, where chromophores (cytochromes, porphyrins and flavoproteins) absorb and convert the heat energy to chemical kinetic energy [55, 56] within the cell. This changes membrane permeability improves mitochondrial signaling with nucleus and cytosol, nitric oxide formation and elavates oxidative metabolism thereby producing more ATP [44, 54, 57, 58,] which further results in suitsble cell function, cell proliferation, pain relief and healing of wound [44, 55, 56]. Below are some of the proposed assumptions that explain LLLT mechanism which includes:

2.6.1.1 Assumption of Singlet Oxygen (¹O₂)

This was based on visible laser light action on RNA synthesis rates in HeLa cells and spectroscopic data for porphyrins and flavins (photo-absorbing molecules which can be reversibly converted to photosensitizers) [59]. The molecular absorption of light is responsible for generation of singlet oxygen ${}^{1}O_{2}$ which leads to stimulation of RNA and DNA synthesis [60, 61].

2.6.1.2 Assumption of Nitric Oxide (NO)

In hypoxic or stressed cells, mitochondrial nitric oxide can bind to Cox, displacing O_2 in competitive mode thus inhibiting respiration especially [62]. And also NO concentration is enhanced under pathological conditions (resulting from activation of NO producing macrophages [63]. It was assumpted that [64, 65] laser irradiation and activation of electron flow in cytochrome c oxidase molecule could reverse the partial inhibition of the catalytic center by NO and thus enhance binding of oxygen and respiratory rate. Increased concentrations of nitric oxide have been reported in cell cultures and animals after LLLT due to its release, from Cox in the mitochondria and from other intracellular stores such as nitrosylated hemoglobin and myoglobin, by the photon energy [66].

2.6.1.3 Redox Properties Change and Superoxide Anion Assumptions

The state of redox in certain chromophores like CuA, CuB or hemes *a* and *a3* in cytochrome c oxidase molecule and the rate of electron flow in the molecule are affected by photo-excitation [36]. It was proposed that low or no cellular response is observed at overall optimal cellular redox potential for the particular growth conditions. A rise in intracellular pH due to irradiation has been measured experimentally both in mammalian cells [67] and in *E. coli* [68].

Reactive oxygen species (ROS) formed as natural by-products of oxygen metabolism, have key roles in cellular signaling [69], regulating synthesis of nucleic acids and protein, activation of progression of cell cycle also and enzymes [70]. In [71] suggested that "activation of the respiratory chain by irradiation would also increase production of superoxide anions, the production of which depends on the metabolic state of the mitochondria" [72].

It was also confirmed that LLLT shifts the overall cellular redox potential in favor of greater oxidation [73] and increased generation of ROS and cell redox activity have been demonstrated [74-76]. These cytosolic changes may consequently induce transcriptional changes (regulation of transcription factors).

2.6.1.4 Local Transient Heating Assumptions

The excited electronic state (by means of light) is converted to heat, as a result causing a local transient rise in the temperature of the absorbing molecules. So this transient increase the temperature of the biomolecules may in turn cause structural or conformational changes and initiate biochemical activities [77].

Remarkably, [78] stated that only one of above reactions occurs upon irradiating and formation of excited electronic states in cells, stating that "it is entirely possible that all the mechanisms proposed above lead to modulation of the redox state of the mitochondria (a shift in the direction of greater oxidation)". However, depending on dose and intensity of the light used, some of these mechanisms may significantly prevail. Experiments with *E. coli* showed that, different mechanisms take place at different laser doses, with photochemical at low doses and thermal at higher doses [53].

2.6.2 Secondary Effect/Reactions or Cellular Signaling

The mentioned primary photoreactions are improved by cellular signaling. A metabolic cascade at cellular level results in various physiological changes including cell membrane permeability [53, 79]. Mitochondrial calcium is released into the cytoplasm thereby changing intracellular calcium levels [80] and thus stimulating cell metabolism and regulation of signaling pathways responsible for processes required for wound repair such as migration of cells, synthesis of RNA and DNA, cell mitosis, secretion of proteins and proliferation of cells [81, 82]. All these events are mediated through cascades of cellular signaling and photosignal transduction [83].

Many researches confirmed that intracellular redox state regulates differents cellular signaling pathways [84, 85]. It is believed that fourteen extracellular stimuli stimulate cellular responses such as proliferation, differentiation, and even apoptosis through cellular signaling pathways. Cellular redox state modulation also affects gene expression through cell signaling mechanisms (via effector molecules like transcription factors, such as nuclear factor kappa B (NF- κ B) and activator protein (AP)-1 [84], and phospholipase A2) [86, 87]. Commonly, cell signaling systems are activated by oxidants, while reductants inhibit upstream signaling cascades, with resultant suppression of transcription factors [88]. Despite similarity in cellular signaling, the resultant cellular responses to irradiation may differ due to variation in modes of regulating transcription factors.

An effort was made to enumerate the extent of irradiation effects as dependent on the metabolic status of *E. coli* cells. A correlation was found between the amount of ATP in irradiated cells and the initial amount of ATP in control cells [16]. Thus, variations in the effects of low level laser at the cellular level are explained by the cellular redox state (and pHi) at the time of irradiation.

2.6.3 Tertiary Effect or Response

Here the effects induced in cells are away from site of secondary reactions [53]. Communication between irradiated and non-irradiated cells, occur through amplified levels of cytokines or growth factors [89]. This boosts immune response by activating T-cells, macrophages and mast cells, with subsequent improved synthesis of endorphins and decline in bradykinin resulting in pain relief [90].

2.6.4 Non-mitochondrial Chromophores as Agent of Metabolic Improvement

Processes that involved in the regulation of redox activities are unabled to occur via the respiratory chain alone. Redox chains containing visible spectra chromophores are the main key structures of regulating metabolic pathways. NADPH-oxidase multi-component enzyme system of phagocytic cells, responsible for non-mitochondrial respiratory burst, is a redox chain that generates ROS in response to microbicidal or other types of activation. Irradiation with 670nm diode laser and other lasres exerted a positive biomodulatory effect on the growth and differentiation of human osteoblasts proliferations as well as others cells [91].

LITERATURE REVIEW

3.0 Low Level Laser Therapy (LLLT)

Low level light/laser therapy (LLLT) is the use of light to promote tissue repair, reduce inflammation, induce painlessness or stimulate cell proliferation etc. Not like many others, LLLT treatments is not an ablating or heating based therapy but rather a photochemical effect which means the light is absorbed and cause a chemical change [92] and is more equivalent to photosynthesis in its mode of action. LLLT also differs from photodynamic therapy (PDT), which employs light indirectly to activate photosensitive dyes to produce bactericidal molecules that kill causing disease microbes.

In contrast, LLLT or photo-bio-modulation uses the achievement of light and light alone to directly kindle host cells in order to reduce inflammation, relieve pain and/or stimulate wound healing. The technique termed low level because the optimum levels of energy density delivered is low and is not comparable to other forms of laser therapy as practiced for ablation, cutting, and thermal tissue coagulation [93].

The biological effects of low level laser therapy have been described in a diverse range of cell and tissue culture systems, animal models, and occasionally in humans. Different cells and tissues have been studied, some normal, some with different disease characteristics. At cellular level LLLT causes adjustments biochemically and bio-energetically, leading to metabolic enhancement, proliferation and maturation of cell, amplified quantity of granulation tissue with decreased inflammatory mediators and enhanced healing process [94, 95].

Furthermore, cellular absorption of laser irradiation results in increased cell metabolism with characteristic stimulation of mitochondrial respiratory chain photoreceptors, changes in cellular level of ATP, release of growth factors, and synthesis of collagen [96].

Replication of DNA, proliferation of cells, enhancement of microcirculation and other cellular processes have been shown to occur between the red and IR wavelength. Low

laser irradiation has also increased growth factors, with subsequent angiogenesis, release of cytokine and increased production of cellular matrix [97, 98].

Both in-vitro and in-vivo experimental studies on LLLT have been underway since 1960s, which led to its approval by U.S. Food and Drug Administration as an important method for hastening cell proliferation and wound healing in early 1990s [99-101].

Low power and doses of laser irradiation have been shown to stimulate in vitro proliferation of fibroblasts [102, 103], keratinocytes [104], 16 endothelial cells [105], and lymphocytes [106]. The proposed proliferative mechanisms involve photostimulation of mitochondrial processes, which enhance release of growth factor, ultimately leading to proliferation of cells.

This study [107] showed a dose dependent enhancement of human gingival fibroblasts proliferation by low level irradiation. This study also [108] showed that low laser irradiation could activate skeletal muscle satellite cells, enhance their proliferation, inhibit differentiation and regulate synthesis of proteins. Furthermore, modulation of matrix metalloproteinase activity and gene expression in porcine aortic smooth muscle cells were evident [109].

However, there is no uniform result in instruments tested, parameters of the laser used like energy density, duration and frequency of exposure [110]. The statement that LLLT may have clinical utility in speed up wound healing is result from its ability to stimulate cell proliferation, cell motility and angiogenesis, while alleviating the inflammatory response. Several studies report LLL-induced cell proliferation, findings are not uniform, perhaps influenced by the variations in cell lines tested, culture conditions and timing of LLL exposure, and differences in LLL fluence, energy, and density.

There is study like [111] that reported LLL stimulated fibroblast proliferation, but decreased similar changes in human bronchial epithelial cells and in a human oral squamous cell cancer (SCC) cell line. In line with this, another study by [112] reported an increased in proliferation and expression of cyclin D1 in LLL-exposed (3 J/cm² to 12 J/cm²) human keratinocytes. In another study, the same authors studied the effects of LLL (2.05, 3.07 or 6.15 J/cm²) on oral dysplastic cells or oral SCC cells. Similar to previous reports, they find out that Akt/mTOR/Cyclin D1-mediated modulation of cell

growth, expression modification of proteins associated with progression and invasion of the cell lines, and pAkt, pS6 and cyclin D1 with production of an aggressive Hsp90 isoform [113]. In the research by [114] reported that LLLI (0.5J/cm² or 1.0J/cm²) on cultured human tongue SCC cell lines, higher proliferation was observed in the two laser treated groups after 24 hours of culture with 0.5J/cm² being more significant.

One study using protein kinase C's as a replacement endpoint showed relation in cell proliferation and apoptosis, the reaction of human lung adenocarcinoma cells to energy levels of 0.8J/cm² or 60J/cm² were compared. While lower energy LLLT induced cell proliferation by activating PKCs which showed PKC activity decreased during apoptosis induced by high fluence laser [115].

Similarly study by [116] found that the best photobiostimulatory dose of LLL was 180mJ/cm² compared to 420–600 mJ/cm² dose bioinhibitory activities. In another study of oral epithelial cells, it was found that in contrast to 20 J/cm², 4 J/cm² resulted in ROS accumulation which did not caused the damaging of DNA and did not induce genomic instability. By comparing the two energy levels in oral keratinocytes, both energy levels contributed to epithelial cell migration through activation of the mTOR signaling pathway [117].

Low-energy laser irradiation using gallium-arsenide semiconductor laser in the study of histopathological rat submandibular salivary glands revealed a results that mitoses of duct epithelial cells without atypia elevated between one and twenty four hours after irradiation, having a greater increased 24 hours as compared with the control. Mitoses of duct epithelial cells are more effeciant in granular ducts, low in striated ducts and still lower in intercalated ducts [118].

Human cells i.e Human gingival fibroblast that is isolated from gingival connective tissue recieved soft laser irradiations showed a higher proliferation activity. High significant differences were observed at 24 hour after irradiation but decreased at 48 and 74 hours in an energy-dependent manner [119]. The proliferation of collagen fibers promoted by laser radiation was also observed in a study by [120] when assessing the therapeutic effect of GaAlAs laser at 63.2 J/cm² on the repair structure of the medial collateral ligament of rats and endothelial cell (EC) proliferation plays a key role in the process of tissue repair.

At different energy fluencies of 1.96, 3.92, and 7.84 J/cm² 809nm using GaAlAs diode laser showed a significantly increased in the metabolic activity of periodontal ligament fibroblasts (PDLFs) which were incubated for three days [121]. A study by [122] found out an increased in fibroblast proliferation in vitro irradiated with infrared LLL irradiation, which can lead to the indication of possible stimulatory effect on wound healing in vivo. The Chinese hamster ovary cells (CHO K-1) that received LLL (830nm; 10mW; 2J/cm²) irradiations showed an increased level of cellular division, as proved by examining the intermediary filaments of the cytoskeleton and the chromosomes [123]. And also by [124] studied osteoblasts that recieved LLLI and found that in proliferation phase the number of osteoblast significantly increased 3 and 5 days after LLL irradiation in comparison to the control.

It was observed that the proliferations of fibroblasts are faster than that of endothelial cells in response to laser irradiation. Using 665 and 675 nm light has higher or maximum proliferation than 810 which inhibit the fibroblast proliferations [105]. Another research by [125] demonstrated the effect of LLLT on the proliferation of human osteoblast-like cells which are the cells derived from human mandibular bone were exposed to GaAlAs diode laser at dosages of 1.5 or 3 J/cm² which were then seeded on titanium discs. At ninety six hours, they found that LLL irradiation put significantly increased in the cell proliferation.

According to the study by [126], the densities of one and three J/cm² of LLLI energies was found to significantly increase the number of mesenchymal stem cells (MSCs) and cardiac stem cells (CSCs) up to 2 and 4 weeks respectively when compared to the control. Another study by [127] assesses the effect of 830nm LLLI on cell proliferation of normal primary osteoblast (MC3T3). The LLLI was performed at 3 different wavelengths and four energies levels of 0.5, 1, 5, and 10 J/cm². One day after LLL irradiation, cell proliferation was measured. Osteoblast proliferation and alkaline phosphatase (ALP) activity in the osteoblast line revealed a significantly increased after the irradiation with 830nm laser irradiation at ten J/cm².

[128] used a diode-based method to generate a similar wavelength to the He-Ne laser (363 nm). They reported that irradiation at 5 J/cm^2 of adipose derived mesenchymal stem cells resulted in enhanced proliferation, viability and expression of the adhesion

molecule beta-1 integrin as compared to control. [129] found that irradiation of gingival fibroblast with LLL (685 nm) for 140 s at 2 J/cm² increased the proliferation as well as the release of bFGF, IGF-1, and IGFBP3 from these cells. Irradiation of bone marrow derived mesenchymal stem cells with 635 nm diode laser (60 mW; 0, 0.5, 1.0, 2.0 and 5.0 J/cm²) significantly stimulated their proliferation and 0.5 J/cm² was found to be the optimal energy density [130].

The research by [131] comfirmed the effect of LLLT as it increased endothelial cell proliferation and migration. Achilles tendon fibroblasts proliferation increased significantly as it irradiated with LLLI, whereas higher laser intensity did not achieve a correspondingly higher cell proliferation effect [74]. In a study of a rat model of disuse atrophy muscle regeneration by LLLI, at the time of the recovery period, rats irradiated daily with (Ga-Al-As laser; 830 nm; 60 mW; total, 180 s). After two-weeks, the percentage of capillaries and fibroblast growth factor levels differed significantly in the laser-treated and the control groups of the muscles. Furthermore, LLL treatment has reasonable effect on the proliferation of satellite cells [132]. The main idea of LLLI to have potentialeffect on cellular proliferation is a wavelength and dosage dependent; however, other important key parameters such as irradiance need to be address [133].

A study by [134] showed that significant increased in the proliferation of Primary fibroblast cell culture from human keloids irradiated with three (3) J LLLI while the 3T3 cell culture revieled no significant difference. Significant decrease in the percentage of the cells was observed in the proliferative phases of the cell cycle that were irradiated with 21 J in the two cell types. These findings support the assumptions that the physiological state of the cells has can have influence to the LLLI results, and high metabolic rate and short cell cycle of 3T3 are not responsive to LLLT.

Human periodontal ligament fibroblasts (PDLFs) received GaAlAs semiconductor diode laser irradiation for ten, twenty and thirty seconds showed an increased in cell proliferation in a time-dependent manner as the cell gradually increased proliferations during 72 hours with no significant difference between treatment and control groups compared within 72 hours, significant increased in PDLFs proliferation was observed between 24 and 48 hours at both 1.97 and 3.94 J/cm² energy fluencies [135].

Human osteoblast-like cells seeded on titanium/zirconia surfaces, were irradiated 3 hours later, the activity of mitogen and ALP activity were increased indicating that LLLT stimulates osteogenic cell proliferation [136]. One study of osteoblastic activity in the rats by [137] found that the cellular doubling time in the proliferative stage at 3-7 days was decreased 24 and 48 h after LLLI by the increased growth of the cells in a culture.

For the study conducted by [138] used 810nm, 50 mW diode laser with 2 different energies (1 J/cm² and 4 J/cm²) irradiate human schwann cells (SCs) for 3 consecutive days. Significant decrease in cell proliferation of the control groups was observed compared with treatment groups. On the seven day, there is significant increase in proliferation in both irradiated and control groups with no significant difference between the laser treated groups.

The photobiostimulatory effect of LLLT is obvicious by enhancing production of some cytokines and growth factors. Laser (685 nm, 25 mW, 14.3 mW/cm², 140 sec, 2 J/cm²) was used to irradiate osteoblasts for for 2 consecutive days. The result showed that the irradiated groups revealed higher proliferation, viability, bFGF, IGF-I, and IGFBP3 expressions than the control group. They came to the conclusion that the biostimulatory effect of LLLT has connection with increased in the production of the growth factors [139].

Another research [140] Nd:Yag laser at different powers (100 mJ, 1.5 W and 150 mJ, 2.25 W) was used to irradiated osteoblasts. There were significant increased in the proliferation of treatment groups compared to the control at 7days. After 14 days, there was no effct on cell proliferation.

ALP activity and LLLT effects on cell proliferation of human osteoblast-like cells (Saos-2) treated with different level of zoledronate, the bisphosphonate, were studied by [141]. Different concentrations of zoledronate were used to treate the cells then irradiated with diode laser (808 nm wavelength, 10 s, 0.25 or 0.50 W). The LLLT was observed to increase the ALP activity and proliferation rate of the cells, while zoledronate reduced both the two. LLLT declined the harmful effects of zoledronate and improved cell function and/or proliferation when applied together. In addition, [142]

found that the proliferation of mouse MSCs was significantly improved after irradiation with 635 nm diode laser.

Some researches have been proved that lasers have been shown to be stimulatory, inhibitory, and or not effective at all. Simply, these observations are due to the experimental set up of the parameters used in the research. One study [143] made an interesting statement that "the magnitude of the laser bio-stimulation effect depends on the physiological state of the cell at the moment of irradiation". Currently, the lack of single well matured and accepted actual explanation of mechanism of low level laser biostimulation complicates the evaluation of the conflicting reports in literature.

There is a study [144] irradiated human umbilical vein endothelial cell (HUVEC) with a 670nm diode laser (power: 10-65 mW cm⁻², dose: 2-8 J cm⁻²) for 6 days. They found a reasonable stimulatory effect of laser irradiation on HUVEC cell proliferation. Doses between 2 and 8 Jcm-2 induced statistically significant cell proliferation. Testing different powes at a constant dose of 8 Jcm⁻², 20 and 65 mW cm⁻² present well pronounced cell proliferation. They came to the conclusion that LLLT influences EC proliferation and this may leads to the increase in angiogenesis and the acceleration of wound healing in vivo.

One study [145] observed that LLLI 670nm and doses of 1.0 and 2.0J/cm² exerted a positive biomodulatory effect on the growth and differentiation of human osteoblasts. The best results were obtained with the dose of $1.0J/cm^2$, which was in agreement with the present findings showing higher proliferation of BMSCs and ADSCs treated with a dose of $1.0J/cm^2$ over period of time.

MATERIALS AND METHODS

4.1 Cell Culture

Human MCR-5 lung fibroblasts (ATCC® CCL171TM) cell line which was isolated from lung tissue taken from a 14 week fetus aborted for psychiatric reason from a 27 year old physically healthy woman was cultured and was used in this experiment in accordance with standard sterilization technique and safety rules maintaining recommended strict aseptic conditions under the supervision and approved protocol of ethic commity of İstanbul Üniversitesi at Deneysel Tıp Araştırma Enstitüsü (DETAE).

4.1.1 MRC-5 Cell Thawing Processes

The biological safety cabinet and all equipments were used in strict aseptic conditions. MCR-5 cells were used in this experiment. The cryopreserved vial of MRC-5 cell line that was stored in liquid nitrogen vapour at -80 °C was placed in 37 °C water bath for 2 min agitation. The thawed cryomedia with DSMO (Dimethyl Sulfoxide) in the vial was added into 15 ml falcon tube containing 10 ml of EMEM (ATCC-formulated Eagle's Minimum Essential Medium with Earle's Salts, with L-Glutamine Cat. No.: MEM-A (500 ml)) and centrifuge at 1500 spin for 2 min. The supernatant was discarded and the pellet of the cells was resuspended in 10 ml medium and centrifugation was repeated once more in order to get rid of DMSO. All of the cells in the pellet were seeded with EMEM containing 10% FBS and the next day medium was refreshed in order to get rid of dead cells (Figure 4.1).



Figure 4.1 Seeding cells in the wells and Subculturing steps

4.1.2 Seeding and Subculturing

After seeding of cells into 75cm^2 culture flasks, cells were attached to the surface of flasks (Figure 4.2). When cells became 80-90% confluent, they were subcultured. Before the subculture, EMEM, FBS, PBS and trypsin were warmed in a 37° C water bath. Medium in the flask was removed by a sterile pipette and then 5 ml of calcium and magnesium free Phosphate Buffered Saline (PBS) was added to remove residual medium. After removal of PBS, 4 ml of pre-warmed 0.25% Trypsin/EDTA (GIBCO) was added to the flask and kept at room temperature for 1-2 min. Then cells were observed under invert microscope (Leica Microsystems CMS GmbH P MAX=5W U=5V DC Type 11090137001). When cells were detached from the surface of the flask, 1 ml of FBS added to the flask to inactivate the function of trypsin.

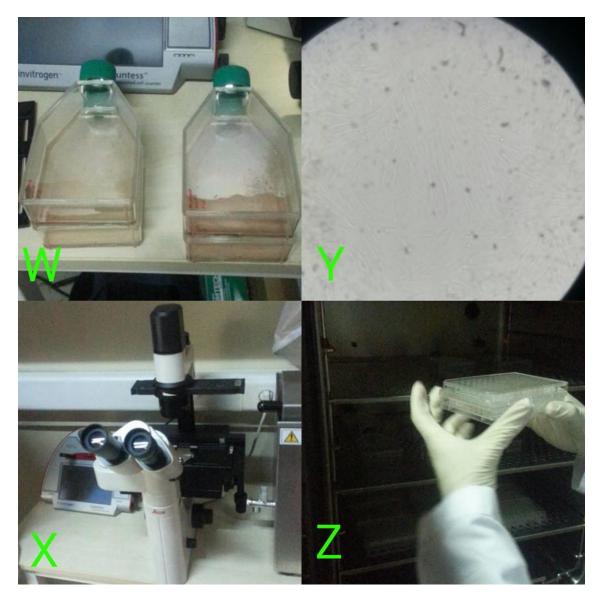


Figure 4.2 W: 75 cm² culture flask, X: light Microscope, Y: Growing cell after subcultured under microscope and Z: an incubator that maintained at 5%CO₂, 37°C with relative humidity

The cells in the flask with trypsin and FBS was transferred into a new 15 ml falcon tube and centrifuged at 1500 rpm for 10 min at room temperature. After centrifugation, supernatant was discarded leaving about 0.5 ml of the cell suspension at the bottom. Pellet was finger mixed and volume was up to 10 ml with EMEM medium in order to remove the remaining any trypsin. Centrifugation step was repeated once more and then cells were counted by hemocytometer. After counting, cells were seeded at density 1 x 10^4 cells/well with 10% FBS containing EMEM for expansion. Subculture of cells was repeated at about 4-5 days intervals.

4.2 Experimental Design and Operations

In this experiment, a laser system set up with three 670 nm emitting diodes, controlled sepaterely was used (Figure 4.3). System specifications is given in Table 4.1 (λ =670nm, 3x400mW 500mw Sony MM Laser Diode 9mm N type 30°C SLD1332V Prophotonix fiber of Fatih University).



Figure 4.3: Laser System: J: Power Meter, K: Laser Beam & Eye protecter and L: Laser system with three 670 nm emitting fiber outputs. M: Laser parameters can be set on the touch-screen.

Laser Parameters					
Laser	3 Diode Lasers				
Wavelength (nm)	670				
Wave Emission	CW				
Power Output (mW)	10, 50 and 100 (used in experiments) (400 mW max)				
Spot Size (cm ²)	0.63				
Fluence (J/cm ²)	1.58				
Power Density (W/ cm ²)	0.0158, 0.079 and 0.158				
Durations (s)	100, 20 and 10 for 10, 50 and 100 mW applications respectively				

Table 4.1 Laser Parameters used

The MRC-5 cell lines were seeded in 96 well plates $(1 \times 10^4 \text{ cells / well})$ in 100 µl medium and incubated in a humid atmosphere with 5% CO₂ at 37°C to settle down overnight. Three 96 well cultured plate seeded with 1×10^4 cells / well designated as plate1, plate2 and plate3 ware used and each plate (Figure 4.4) contains A, B, C and D groups, each with six replicates wells. Group A (Light1+Cells) received LLLI of 10 mW power output for 100s, Group B (Light2+Cells) received 50 mW for 20s, Group C (Light3+Cells) received 100 mW for 10s thus achieving a single dose of 1.58J/cm² each and Group D (Only Cells) served as control group and received no LLLI as showed in Figure 4.4. Plate1, plate2 and plate3 were immediately incubated (in humid atmosphere with 5% CO₂ at 37°C) after the treatment for 3hours, 6hours and 24hours respectively.

А	А		D	D		С	С	
А	А					С	С	
А	А					С	С	
			В	В				
			В	В				
D	D		В	В		D	D	

Figure 4.4 Groups distribution on 96 wellplate with empty wells between the groups

The irradiations were done spot by spot to cover the entire cell well area with the tip of the optical fiber positioned above the cultured well during all laser applications and each group was surrounded with empty well to avoid scattering (Figure 4.4). The spot size of the laser beam was measured as 0.63 cm² and laser power was checked with an energy meter (S121C Standard Photodiode Power Sensor, Si, 400 - 1100 nm, 500 mW, PM200 Optical Power and Energy Meter Thorlabs). Continuous mode of irradiation was applied and the plates were not covered during the irradiation process which was performed in the room temperature. All the experiments included a control group of cells grown under the same conditions but not irradiated and the parameters were set after thorough review of related literature as reported above.

4.3 Cell Viability

The measurement of cell viability is one of the most important tests in different forms of cell culture, which tests the number of healthy cells in a sample. Among the methods apply to determine cell viability, the reduction of different kinds of tetrazolium salts etc.

WST-1 assay is based on the cleavage of the tetrazolium salt WST-1 to formazan by cellular mitochondrial dehydrogenases (Figure 4.5) that lead to an accurate cell prolifearion result. The product formazan produced by WST-1 is soluble which leads to a wider linear range and higher sensitivity with the standard incubation time of WST-1 time is 2 hours. Single addition of the reagents can reflect the effect of the testing materials at different time points on the trend of relative cell viability [145A].

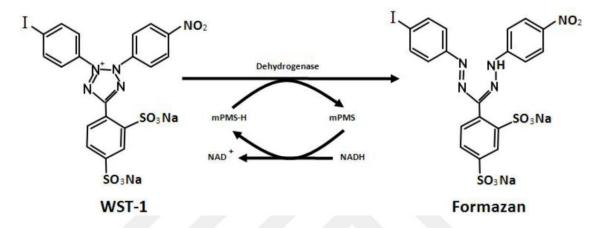


Figure 4.5 Schematic mechanism of the WST-1 reduction [145A]

4.3.1 Application Protocol

WST-1 (Roche) cell proliferation assay was used to determine the number of healthy cells in control and laser treated groups of this experiment. The reagents was taken from its storage (-20 °C) and thawed for two minutes using water bath. After incubating the laser treated and control groups in 96 well cultured plate designated as plate1, plate2 and plate3 for 3hours, 6hours and 24hours respectively. 10µl of WST-1 reagent mixtures was added to each well plate ($1x10^4$ cell/well) in 100µl of EMEM. The cultured plate was gently shaked for one minute in order to ensure the homogeneousity of the colour and was incubated for two hours at $37^{\circ}C$, 5% CO₂ incubator.

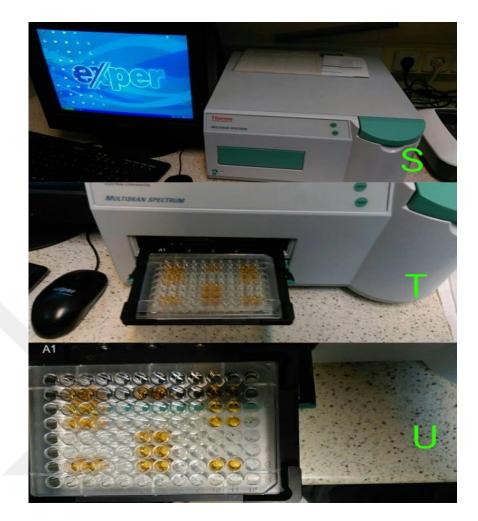


Figure 4.6 Analysis of Cell viability S: Microplate Reader System, T: Side View, U: Top View

After two hours of incubation, the plate was placed in microplate reader (Thermo Electron Corporation, Multiskan Spectrum) (Figure 4.6) to measure the absorbance at 450nm wavelength. The same procedure was done for all plates. The cell viability percentage in each group was calculated by comparison to that of the control group.

4.4 Statistical Analysis

ANOVA (Analysis of variance) and paired comparison analysis followed T-test were employed to test for statistical differences in the set of data at p equal to 5% (p=0.05) level of significance for laser treated and non laser treated groups at three differents incubation hours.

CHAPTER 5

RESULTS AND DISCUSSIONS

5.1 Results

Below are the graphical illustrations of the results, the lowest proliferation was observed for the control group (no laser treatment) at all studied time frames when compared with irradiated groups.

The comparison of the three laser powers showed a tendency towards higher cell proliferation in the groups treated with 50 mW at 3 and 6 hours, followed by 10 mW in 24 hours (Figure 5.1 to 5.4). Inorder to find out where are the significant differences are, we conducted paired comparison (t-test) of six possible pairs (AxD, BxD, CxD, AxB, AxC and BxC groups). A significant difference in cell proliferation was observed between the control groups and the groups treated with the three power output 10, 50 and 100 mW after 3, 6 and 24 hours respectively with all the powers stimulating cell growth. No significant difference is observed in cell proliferation in the 4 possible pairs compared as AxC in 3 hours, AxD & AxC in 6 hours and finally BxC in 24 hours Groups (Figure 5.5 to 5.10).



Figure 5.1 Mean proliferation of MRC-5 human fetal lung fibroblasts submitted or not submitted to laser irradiation over 3 hours incubation time

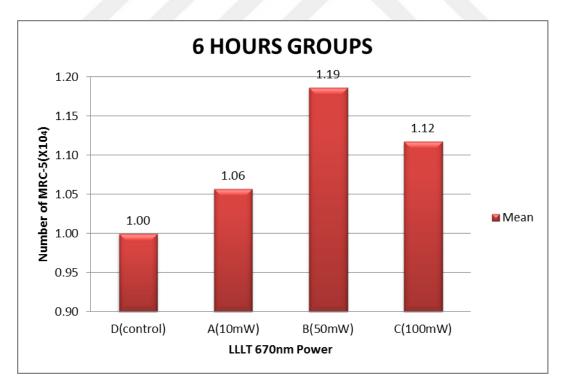


Figure 5.2 Mean proliferation of MRC-5 human fetal lung fibroblasts submitted or not submitted to laser irradiation over 6 hours incubation time.

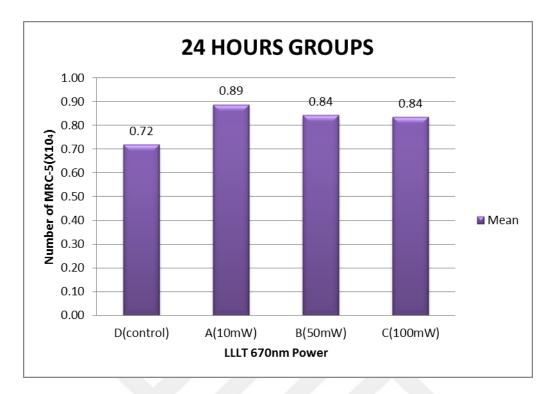


Figure 5.3 Mean proliferation of MRC-5 human fetal lung fibroblasts submitted or not submitted to laser irradiation over 24 hours incubation time.



Figure 5.4 Growth curve of MRC-5 human fetal lung fibroblasts submitted or not submitted to laser irradiation over time (incubation hours).

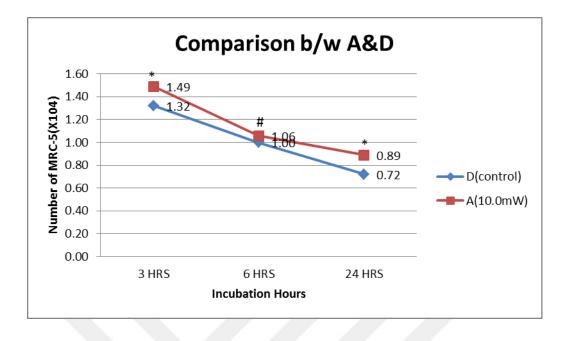


Figure 5.5 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between A (10.0 mW) and D (control) groups over times (incubation hours), * donates statistical significant difference (SSD) while # donates no SSD between A vs D.

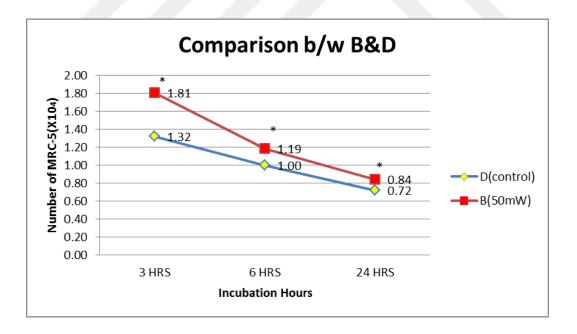


Figure 5.6 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between group B (50.0 mW) and D (control) over times (incubation hours). * donates statistical significant difference (NSS) between B vs D.

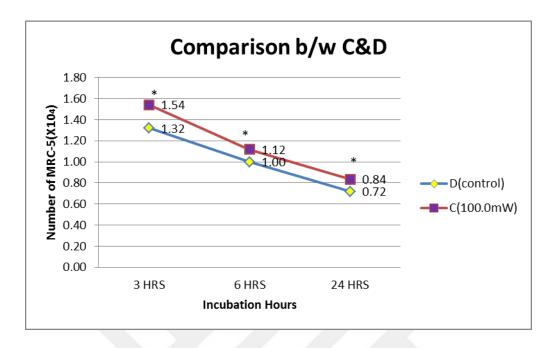


Figure 5.7 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between group C (100.0 mW) and D (control) over times (incubation hours). * donates statistical significant difference (NSS) between C vs D.

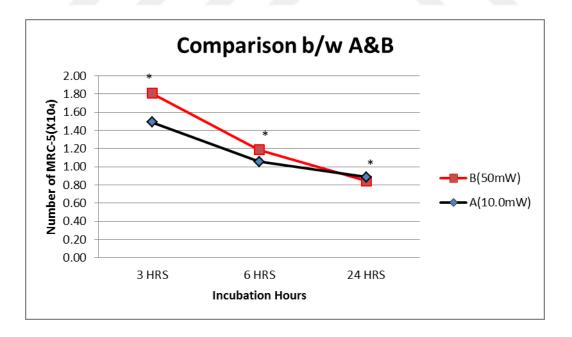


Figure 5.8 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between group A (10.0 mW) and B (50.0 mW) over times (incubation hours). * donates statistical significant difference (NSS) between A vs B.

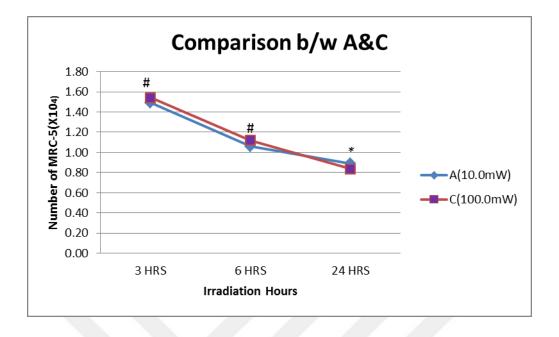


Figure 5.9 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between group A (10.0 mW) and C (100.0 mW) over times (incubation hours). * donates statistical significant difference (NSS) while # donates no SSD between A vs C.

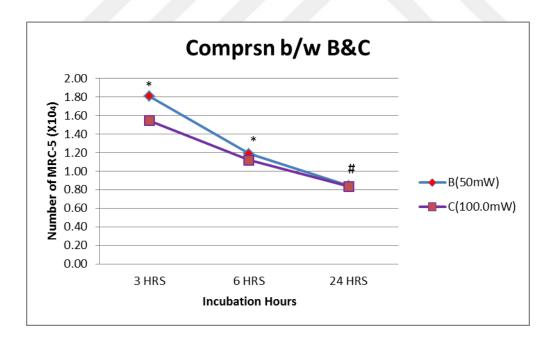


Figure 5.10 Growth curve of MRC-5 human fetal lung fibroblasts, comparison between group B (50.0 mW) and C (100.0 mW) over times (incubation hours). * donates statistical significant difference (NSS) while # donates no SSD between B vs C.

5.2 Discussion

Biostimulation and differenciation can be achieved using LLLI to different types of cells as reported by authors [146, 147, 148, 119, 149]. Sometimes, biostimulation is inhibited due to the effect of variety of factors in the process [150]. As a result, biostimulation using *in vitro* depends on laser-related parameters such as power, dose, time and also wavelength of irradiation [119, 149, 151], type of irradiated cell [105] and the physiological characteristics of the cells during irradiation [149, 151]. Thus, laser light mode of interaction with cells and tissues can lead to stimulation or inhibition of cell proliferation.

Pinheiro et al. observed that absorption and spreading of light are greater due to the lack of an optical barrier by applying lower doses for the irradiation to mucosa and skin wounds [152]. Many authors revieled that in vitro studies normally reflect the same conditions as observed in open wounds, i.e., the lack of an optical barrier, and lower doses are, thus, indicated in the case of biostimulation. On the basis of this hypothesis, doses of 1.58J/cm² with three different power output 10, 50 and 100 mW were used in the present study because the objective was to stimulate the proliferation of MCR-5 lung fibroblasts (ATCC® CCL171TM) cell line. One research confirmed that, a dose or power increase the damages of photoreceptors, which reduces the biomodulatory effect of the laser as a result of the inhibition of metabolism and consequent cell death [153]. Another study [119] supported this assumption by revieling that laser irradiation using a dose (like 4.0J/cm²) trigger cell proliferation but high doses caused negative effect on this biological system/process. An in vitro study was conducted and confirmed the enhancement of HUVEC proliferation that received LLLI at the wavelength range 670 nm and doses of 2, 4, 8 J/cm² [158]. Wavelengths of 600 to 700nm were used when the objective was to stimulate cell proliferation [155]. Increased cell proliferation and viability was observed in human ADSCs irradiated with diode laser (5.0J/cm²) [147]. These results agree with the present findings that show an increased number of cells. Researchers agree that lower doses decrease the risk of cell damage and encourage the proliferation, without causing any change in the initial characteristics. Therefore LLLT showed a power output-dependent effect in the present study, as specified by the higher proliferation rate of MCR-5 lung fibroblasts (ATCC® CCL171™) cell line when irradiated with a power output of 50 and 10 mW compared with 100mW. Another study confirmed that LLLI using a wavelength of 670nm and doses of 1.0 and 2.0J/cm² with output power 20 and 65 mW showed a positive biomodulatory effect on the proliferation of human osteoblasts [145]. The best results were obtained with the dose of 1.0J/cm², which was in agreement with the present findings showing an increased proliferation of MCR-5 lung fibroblasts (ATCC® CCL171TM) cell line treated with a dose of 1.58J/cm².

A study investigating the effect of LLLI at different wavelengths (625, 635, 645, 655, 665, 675, and 810nm) on two types of cells (endothelial and fibroblasts) evaluating their cell proliferation rates after 24 hours of culture. Moore P *et al.* found the effective result in both cells proliferations and wavelengths except for the wavelength of 810nm [105]. The similar result was reported regarding the proliferation of fibroblasts by Evans DH *et al.* [156] using 632.8 and 830nm wavelengths in the evaluations. They concluded that effective biostimulation of fibroblast proliferation for cells treated with those wavelenths interfare with the cell response. The wavelength used in the present study (670nm) was within the range that was employed in biostimulation studies, and, as reported in the literature, we observed a positive effect on the proliferation of the cells tested.

The effect of LLLI on the proliferation of BMSCs was investigated and no significant difference was found between the groups after 7 days [148]. These results differed with the present study in which significant differences in the proliferation rate of MRC-5 were observed between the irradiated and control groups. This is due to the some factors that involved in the experimental setup which may include [148] the dose used (4.0J/cm²) and wavelength (808nm) of the study design. As mentioned earlier, inhibitory effects on cell proliferation may occur as a result of using wavelengths outside the range of 600 to 700nm and high irradiation doses [149, 151, 155]. These results agree with the suggestion of some investigators that the effect of LLLT is directly related to the irradiation power, dose, physiological state of the cell line, and wavelength used [127, 149].

Type of cell line that is used is a factor that influences the effect of laser therapy. Because of this, a study evaluated the effect of diode laser at a dose of 5.0J/cm² on the

proliferation of human ADSCs and used cell line that was obtained during surgery and a commercial cell line and got different results. Commercial cell line showed no significant difference in proliferation at any of the studied time points (24, 48, and 72 hours).



CHAPTER 6

CONCLUSIONS AND RECOMMENDATIONS

6.1 CONCLUSION

The present study showed that low-level laser irradiation promoted the proliferation of MCR-5 lung fibroblasts (ATCC® CCL171TM) cell line compared to control group. The cell morphology is fibroblast-like thus present a low yield and low proliferation rate, low-level laser irradiation may be a useful tool for enhancing such cells through multiples subculturing reducing high cost and difficult to obtained. In this respect, laser therapy permits a significant increase in the initial number of MCR-5 lung fibroblasts, thus increasing the number of regenerative cells therefore enhancing healing processes.

6.2 **RECOMMENDATIONS**

For better understanding, it is good to ensure that correct protocols are developed for laser therapy and should include the use of appropriate power output, wavelength, dose, power density, irradiation time, as well as frequency and number of sessions as these parameters may have an influence on cell proliferation leading to achievement of good results and also avoiding controversies and empirical conclusions. However, further studies are needed to standardize the laser parameters and to test other cell types to improve the yield of cells in culture.

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APPENDIX A

Groups	Control	Treatment				
Subgroups	D	А	В	С		
Number	6	6	6	6		
Power (mW)	-	10	50	100		
Power Density (W/cm ²)	-	0.01158	0.079	0.158		
Energy Density (J/cm ²)	-	1.58	1.58	1.58		
Laser Mode	_	CW	CW	CW		
Duration (S)	_	100	20	10		

Experimental groups and Application protocol

Appendix B

	STAT FOR MEAN ± STANDARD DEVIATION									
	Control Group (D)									
	PR of D	D-Mean	Y=(D- Mean)2	Variance ΣY/n	$\frac{SD}{\sqrt{\Sigma Y/n}}$					
3 Hours	1.321	-1.238	1.532	2.450	1.565					
6 Hours	0.999	-1.560	2.433							
24 Hours	0.719	-1.840	3.385							
n	3.00									
Σ	3.039		7.350							
Mean	2.559									

STAT FOR MEAN ± STANDARD DEVIATION									
Group A									
	PR of A	A-Mean	Y=(A- Mean)2	Variance ΣY/n	$\frac{SD}{\sqrt{\Sigma Y/n}}$				
3 Hours	1.490	0.346	0.119	0.413	0.642				
6 Hours	1.056	0.088	0.007						
24 Hours	0.888	1.056	1.115						
n	3.00								
Σ	3.434		1.241						
Mean	1.144								

Group B								
	PR of B	B-Mean	Y=(B-Mean)2	Variance ΣY/n	$SD \sqrt{\Sigma Y/m}$			
3 Hours	1.807	0.529	0.279	0.159	0.398			
6 Hours	1.185	-0.093	0.008					
24 Hours	0.842	-0.436	0.190					
n	3.00							
Σ	3.834		0.477					
Mean	1.278							
Mean	1.278							

STAT FOR MEAN ± STANDARD DEVIATION Group C								
3 Hours	1.542	0.378	0.142	0.084	0.289			
6 Hours	1.117	-0.047	0.002					
24 Hours	0.835	-0.329	0.108					
n	3.00							
Σ	3.494		0.252					
Mean	1.164							

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